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Review

# Multiscale requirements for bioencapsulation in medicine and biotechnology

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# ABSTRACT

Bioencapsulation involves the envelopment of tissues or biological active substances in semipermeable membranes. Bioencapsulation has been shown to be efficacious in mimicking the cell's natural environment and thereby improves the efficiency of production of different metabolites and therapeutic agents. The field of application is broad. It is being applied in bioindustry and biomedicine. It is clinically applied for the treatment of a wide variety of endocrine diseases. During the past decades many procedures to fabricate capsules have been described. Unfortunately, most of these procedures lack an adequate documentation of the characterization of the biocapsules. As a result many procedures show an extreme lab-to-lab variation and many results cannot be adequately reproduced. The characterization of capsules can no longer be neglected, especially since new clinical trials with bioencapsulated therapeutic cells have been initiated and the industrial application of bioencapsulation is growing. In the present review we discuss novel Approached to produce and characterize biocapsules in view of clinical and industrial application. A dominant factor in bioencapsulation is selection and characterization of suitable polymers. We present the adequacy of using high-resolution NMR for characterizing polymers. These polymers are applied for producing semipermeable membranes. We present the pitfalls of the currently applied methods and provide recommendations for standardization to avoid lab-to-lab variations. Also, we compare and present methodologies to produce biocompatible biocapsules for specific fields of applications and we demonstrate how physico-chemical technologies such as FT-IR, XPS, and TOF-SIMS contribute to reproducibility and standardization of the bioencapsulation process. During recent years it has become more and more clear that bioencapsulation requires a multidisciplinary approach in which biomedical, physical, and chemical technologies are combined. For adequate reproducibility and for understanding variations in outcome of biocapsules it is advisable if not mandatory to include the characterization processes presented in this review in future studies.

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# 1. Introduction

Bioencapsulation involves the envelopment of tissues or biological active substances in a semipermeable membrane to protect the enclosed biological structures for potential hazardous processes in the direct environment. The field of application of bioencapsulation is broad. In plant cell cultures [1–3], bioencapsulation has been shown to be efficacious in mimicking the cell's natural environment. Thereby bioencapsulation improves the efficiency of production of different metabolites for industrial application. For fermentation [4–8] bioencapsulation is being applied for enlarging the cell density, aroma and capacity of the systems. Additionally during fermentation it avoids washout of the biological catalysts

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from the reactor. Bioencapsulation also has a pertinent application in medicine. It is, for example, applied to protect biological active substances or cells such as probiotica to the deleterious biological environment [9-12] and for delivery in specific sites such as the colon [13,14]. A relatively large group of researchers apply bioencapsulation for the creation of a bioartificial organ [15]. In this application, therapeutic cells are encapsulated in membranes that protect the cells against antibodies and cytotoxic cells of the host immune system. This immunoisolation by encapsulation has a number of important benefits for clinical application of transplantation. First of all, it avoids the use of systemic and permanent immunosuppression. Immunosuppression has serious side effects such as a higher chance for malignancies and frequent infections. Another benefit is that encapsulation allows for successful transplantation of cells from nonhuman origin, i.e. xenografts, which could be a mean of overcoming the obstacle of limited supply of donor tissue [16]. The principal applicability of the technology has been shown for the treatment of a wide variety of endocrine diseases, including anemia [17], dwarfism [18], hemophilia B [19], kidney [20] and liver [21] failure, pituitary [22] and central nervous system insufficiencies [23], and diabetes mellitus [24].

During the past decades many procedures to fabricate capsules have been described. Unfortunately, most of these procedures are dedicated to the technology of the production process but lack an adequate documentation of the characterization of the capsule. As a result many procedures show an extreme lab-to-lab variation and many results cannot be adequately reproduced. The characterization of capsules can no longer be neglected, especially since new clinical trials with bioencapsulated therapeutic cells have been initiated [25] and the industrial application of bioencapsulation is growing. During recent years many technologies have been described to characterize capsule properties. In the present review we discuss these technologies in view of clinical and industrial applications.

#### 2. Polymers for encapsulation

Producing a microcapsule for envelopment and protection of biologically active substances or cells starts with selection of an adequate encapsulation material. The majority of materials used in microcapsules are polymers, either naturally occurring or synthetic. A major pitfall in the field is the absence of guidelines for documentation of the characteristics of the materials applied. It is mandatory that this documentation will be included since it is now widely accepted that the characteristics of the polymer is a dominant factor in determining the capsule properties.

Several characteristics should be taken into account for considering polymers for formation of microcapsules. The polymer selection starts with the description of chemical composition of the monomeric units. The amount and character of functional groups contained in monomer units (one type of monomer unit in case of homopolymers, two and more types of monomer units in case of copolymers) define the primary structure of polymers. The chemical composition of monomer units gives rise to various interactions such as hydrogen bonding, electrostatic interactions, and hydrophobic interactions, which are important for intra- and intermolecular interactions. These interactions are responsible not only for the effects potentially originating from secondary, tertiary, or quaternary structures but also for the interactions that lead to formation of microcapsules. The most common principle used for microcapsule formation by polyelectrolyte and ionotropic complexation represents a typical example. Since the variability in the chemical character of monomer units is virtually infinite, application of well-characterized polymers in terms of chemical composition is critical in order to understand and control the microcapsule properties and performance.

In addition to the chemical composition, the molecular weight characteristics should be part of the conventional documentation. This includes identification of weight number and average molecular weights ( $M_w$  and  $M_n$ ), and polydispersity  $M_w/M_n$ . The latter characterizes the molecular weight distribution. The molecular weight averages and molecular weight distribution can be measured by various techniques. Conventionally, static light-scattering, viscometry, and size-exclusion chromatography are used to determine the molecular weight averages. The molecular weight distribution is most typically determined by size-exclusion chromatography, although the mass spectrometry techniques have been advancing to assess the molecular weight distribution of synthetic [31] and natural [32] polymers. Molecular weight characteristics are linked to the viscosity and other rheological properties of the polymer solution, which are important for the process of microcapsule formation. The rheological properties are affected by temperature and concentration of the polymer, and by ionic strength in case of polyelectrolytes, which all should be specified for the materials applied in encapsulation.

There are some additional items that should be documented in specific applications, e.g., for medical application it is mandatory to have information on the purity degree of the polymer. At least the endotoxin content, the microbial contamination, and the protein content should be specified and documented.

What the above-mentioned measurements imply for application can be most adequately illustrated with an example. We will do so with alginate which is one of the most dominantly applied polymers in encapsulation. Alginates are natural unbranched binary copolymers of  $1 \rightarrow 4$  linked ß-D-mannuronic acid (M) and  $\alpha$ -L-guluronic acid (G) (Fig. 1A). The alginate composition and sequential structure together with its molecular weight are essential characteristics in determining the capsule properties and functionality. High-resolution NMR is applied to determine the composition and sequential structure of alginates (Fig. 1B).

The molecular weight is mostly determined from intrinsic viscosity measurements or size-exclusion chromatography using light-scattering detection. As alginates do not have any regular repeating unit, the sequential structure is not only determined by the monomer composition (monad frequencies) alone, but also by measurements of diad and triad frequencies. The four diad (nearest neighbor) frequencies ( $F_{GG}$ ,  $F_{GM}$ ,  $F_{MG}$  and  $F_{MM}$ ) and the eight possible triad frequencies ( $F_{GGG}$ ,  $F_{GGM}$ ,  $F_{MGG}$ ,  $F_{MGM}$ ,  $F_{MMM}$ ,  $F_{MMG}$ ,  $F_{\text{GMM}}$  and  $F_{\text{GMG}}$ ) can be measured by NMR techniques [26–28]. From the frequencies we can estimate the average length of blocks of consecutive G units  $(N_{G>1} = F_G - F_{MGM}/F_{MGG})$  and M units  $(N_{M>1} = F_M - F_{GMG}/F_{MMG})$ . Recent development in the field of polysaccharide sequencing allows for an even more detailed characterization. Nowadavs we can assess the true reconstruction of the block structure of alginates. This is done by the use of specific lyases and subsequent analysis of the digest. The digest is fractionated by SEC and the molecular mass and composition of each fraction are then analyzed with NMR and ESI-MS (low molecular weight fractions) or HPAEC-PAD (MALDI-ToF) for the high molecular mass fractions. This latter of course is not yet routinely applied for characterization of alginates for encapsulation.

Since the purity degree of the alginate has been shown to determine the biocompatibility of alginate-based capsules [29,30] it is mandatory to provide details on the purity of this polymer. According to FDA requirements for device implantations, the content of endotoxin must be below 350 EU per patient (below 15 EU per patient for CNS applications). As the chemical properties of endotoxins are very similar to alginates, their removal has been a challenging task but purified alginates with a specified endotoxin



**Fig. 1.** Structure of alginate. A: β-D-mannuronic acid (M) and α-L-guluronic acid (G), with most probable ring confirmation: M: <sup>4</sup>C<sub>1</sub> and G: <sup>1</sup>C<sub>4</sub>. B: <sup>1</sup>H-NMR spectra of alginate from *Laminaria hyperborea* stipe.

content below 100 EU/g are now commercially available. For Good Medical Practice (GMP), alginates must be characterized by validated methods and every product batch must be characterized and documented with its individual laboratory certificate. Characterization parameters for alginates to be used in biomedical and tissue engineered medical products are now thoroughly described in the ASTM guide F 2064 (American Society for Testing and Materials) of the ASTM Book of Standards.

Other polymers in addition to sodium alginate have been successfully applied in encapsulation research [33]. The polymers involve various polyelectrolytes of anionic (cellulose sulfate, chondroitin sulfate, polyacrylic acid) and cation (poly-L-lysine, poly-L-ornithine, chitosan, poly(methylene-co-guanidine), polyvinylamine) nature as well as non-ionic polymers (polyvinyl alcohol, poly(hydroxyethyl methacrylate-co-methyl methacrylate), polyethylene glycol). It is viewed as a positive trend that researchers recently dedicate much more attention to characterization of these materials used for capsule formation than in the past. Thus, the encapsulation protocols provide at least one of the molecular weight averages, chemical composition in case of copolymers and degree of substitution in case of chemically modified polysaccharides. Often, the lot number is another important parameter to be reported, which can help tracking the properties of the commercial polymers in order to improve the labto-lab reproducibility.

# 3. Permeability properties

Encapsulation is applied to protect the enclosed biological materials for deleterious effects of substances or processes in the immediate vicinity of the capsules. This protection is usually accomplished by restricting the diffusion of deleterious molecules by applying semipermeable membranes. The permeability of the capsules is determined by the desired control over both the sizebased exclusion and the rate of diffusion of the molecules, which either have to or must not permeate the membrane. Before discussing the means to measure the permeability properties, it is essential to shortly discuss the factors determining the diffusion characteristics of the capsules since this rationalizes the application of the presented technologies. This will be done with the hydrogel as an example since this is the most commonly applied capsule structure with complicated diffusion characteristics.

Diffusion and permeability properties of hydrogels are determined by at least four factors. The first is the obstruction effect caused by the presence of impenetrable slowly moving polymer chains that increase the path length for diffusion. The second process is the hydrodynamic drag at the polymer interface due to polymer-solvent and polymer-solute bonds during the solute diffusion. The third is the different extent of heterogeneity of the membrane material with fluctuation of diffusion properties across the membrane material. Finally, residual charges, presence of counter ions, hydrogen bonds, polar and hydrophobic interactions of the membrane material will affect the diffusion of solute exhibiting similar interactive groups. This is especially essential in diffusion of biological molecules.

For assessing and expressing the diffusion and permeability of capsules, two factors are of main interest. The first factor that is relevant for expressing the diffusion and permeability of capsules is the rate of solute diffusion, which is reflected in the mass transfer, permeability, and diffusion coefficients. The second one is represented by the membrane exclusion properties considering minimum size of a solute completely excluded by the capsule membrane. This is usually referred to as the exclusion limit or molecular weight cut-off (MWCO). This is related to the membrane pore size. It is important to emphasize that this parameter is not connected with the solute molar mass. It is determined by the size and shape. The MWCO and the rate of diffusion of solute are obviously connected and are of equal importance for quantification of the permeability properties of a semipermeable membrane. Nevertheless, the vast majority of studies only characterize the MWCO to quantify the diffusion properties. This is not without consequences since it does not adequately predict the diffusion properties when other solutes are applied. This is especially true for the hydrogel-based membranes since these materials show large fluctuations in chemical composition, local viscosity, density, interactions with solutes as well as non-uniformity in pore sizes and their distribution across the membrane [34,35].

### 3.1. Selection of solute for quantifying permeability

Many experimental techniques to assess the permeability properties of capsules have been described during the past two decades. These techniques are comprehensively compiled in a number of review articles, for example by Schuldt and Hunkeler [36] and Uludag et al. [37]. Which technique is most suitable for a specific application depends on the type of solute that is applied for measuring permeability. The selection of the technique starts with choosing the solute type, which typically involves proteins, dextrans, and pullulans. In the medical field, the permeability of capsules to IgG is considered as the most important criterion since it is assumed to predict the immunoprotective properties of the capsules after implantation in humans. Not surprisingly, different techniques for quantifying IgG permeability have been developed such as diffusion of radiolabeled IgG [38], fluorescently labeled IgG [39] or entrapping radiolabeled IgG or other relevant proteins inside the capsules [40]. Others, however, prefer to quantify diffusion by applying neutral polysaccharides such as dextrans and pullulans since it is fast and reliable. The obtained information from neutral polysaccharides can also be applied to calculate the permeability for specific proteins by applying the universal calibration principle, which allows for mutual recalculating of viscosity radius and molecular weight for respective polysaccharide and protein [41]. It is recommended, however, to verify whether the calibration principle applies for a specific capsule since theoretically an interaction of proteins with the membrane is more likely to occur than with polysaccharides.

During recent years many other relevant solutes have been proposed for quantifying permeability. Mostly these solutes were chosen because they are playing an essential role in the functionality of the capsule. These solutes include glucose, glycerol, Vitamin B12, etc. [42,43]. The solutes may be applied either unlabeled but the preference is for the radio- and fluorescent-labeled solutes to increase sensitivity and specificity of the applied techniques.

#### 3.2. Quantification of permeability

Many different techniques are available to determine the diffusion properties of solutes in semipermeable membranes [36,37]. Before discussing these techniques, it should be mentioned that the overall permeability of a membrane is determined by a number of capsule properties. It has been shown that the rate of solute diffusion is described by the pore size, the pore size distribution and the chemistry of the membrane and solutes [42,44–47]. In addition, the importance of the membrane thickness for the velocity of solute diffusion was recently shown in studies on diffusion properties of a few micrometer thick nanoporous membrane with uniform pores microfabricated of silicon [48,49] and, more recently, alumina [50,51]. It is therefore advisable to document all these factors including the membrane thickness in studies on semipermeable capsules.

The applied technique for measuring permeability as such depends on the methodology used to quantify the chosen solute. The most commonly applied techniques are spectroscopy techniques (fluorescence, UV–VIS), measurement of radioactivity, size-exclusion chromatography with concentration-sensitive detector, and protein assay kits. Determination of solute permeation can be either in diffusion into the capsules (ingress) or from the capsules (egress) [36]. The results of these experiments can be obtained under equilibrium conditions providing the information on MWCO or at different times until reaching the equilibrium, which results in determination of the transport coefficients.

A technique that may be developed into a widely applied methodology for measuring the permeability of microcapsules is the inverse size-exclusion chromatography [40,41]. The advantage of this technique over the others is that it not only provides information on the, MWCO but also on the pore size distribution (Fig. 2). In this technology, microcapsules are used as the column packing of which the calibration curve with slope (pore size distribution) and exclusion limit (MWCO) are determined simultaneously.

From the above follows that diffusion of the chosen solute, the pore size, the pore size distribution, the chemistry of the membrane and solutes, and the thickness of the membrane are essential for describing the permeability properties of a capsule. Unfortunately, these items are only rarely documented. For that reason it is anno 2009 difficult if not impossible to compare permeability results between different laboratories.

## 4. Mechanical resistance of microcapsules

A capsule should have a sufficient mechanical resistance to withstand the various forces during the whole duration of application. Up to now, mechanical stability did not gain too much attention by the scientific community since it is technically not too advanced to increase the mechanical resistance of microcapsules. Increasing the strength and resistance of the capsules will also increase the durability of the transplant and consequently the drug release time period. However, can this be done without a drawback on other capsule parameters? The answer is no. Increasing the mechanical stability by increasing for instance the membrane thickness of a capsule may influence other important parameters of the capsules such as permeability and intracellular microenvironment [52]. The challenge is therefore not to increase the stability but to determine what mechanical resistance is required for a specific application without changing other relevant capsule characteristics.

The required mechanical resistance for in vivo application of encapsulated therapeutic cells has been studied in more detail than for other fields of application. The required mechanical stability for encapsulated therapeutic cells depends on the proposed site of implantation [53]. It has been shown with alginate-based



**Fig. 2.** A classical example of inverse size-exclusion chromatography. Filled circles represent measured data points of chromatography partition coefficient  $K_{SEC}$  as a function of molecular weight of testing standards (pullulans) used to test for permeation to the microcapsules forming the column packing. Full line is the Boltzmann fit to the experimental data, of which the first derivative (dashed line) represents the pore size distribution. The exclusion limit of the column packing corresponds to the MWCO value of microcapsules.

microcapsules that they should have a higher mechanical stability in the peritoneal cavity than in the stratium or subcutaneous space. Other important factors that influence the required mechanical stability is the type of cells applied [54–56]. At the moment, there are no guidelines for the mechanical resistance capsules should have in the various applications. Lacik reported that the rupture load from a few grams to tens of grams per capsule for intraperitoneal application [33] should be in the sufficient range. This, however, holds for empty capsules and not for cell containing capsules.

Up to now, broken capsules in explants from recipients are used as a rough indication that the mechanical stability of the capsules should be increased. The approach to accomplish such increase without interfering with other important capsule parameters depends on the following factors: the type of biomaterials used for the elaboration of the polymer matrix and membrane [54–56], the type of gelling ion [39], the type of cell, and the selected encapsulation technology. These factors have a mutual influence on the resistance as will be illustrated with alginate-based capsules as an example. The mechanical resistance of an alginate-based capsule depends on the ionic linkages between the gelling ion (usually calcium) and alginate block structure. However, in physiological solutions and in vivo conditions, the calcium-alginate beads are sensitive for chelating and non-chelating agents such as phosphate, sodium and potassium ions, which provoke the osmotic swelling of the beads and their final rupture [57]. To increase the stability of calcium-alginate beads, a polycation is often added [24]. The latter will increase the stability of the encapsulation system due to the polyelectrolyte complex between the alginate and the polycation. Some report mechanical stability problems with this approach. The electrostatically linked complex might still compete with other charged molecules in the environment, limiting the long-term stability of the microcapsule [58]. A possible approach to overcome such a problem is to improve the mechanical characteristics of the alginates [59,60] or to design novel covalently reinforced and photo-crosslinked capsules [61,62].

The foregoing should not be interpreted as a suggestion that hydrogels made of alginate are not mechanically stable enough to allow application for long periods. In general, hydrogels used for cell encapsulation purposes are likely to contain the desired mechanical rigidity (resistance to deformation) and toughness (resistance to fracture by being pliable) to structurally protect enclosed cells. The mechanical properties of the gels are controlled by both the polymer concentration and the molar ratio between polymers and crosslinking molecules [63]. In fact, reducing the distance between the crosslinks and increasing the polymer concentration led to an increase of the mechanical rigidity in hydrogels [64]. Interestingly, unlike other hydrogels formed from covalent crosslinking, calcium crosslinked alginate hydrogels permit increases in both the rigidity and the toughness with higher crosslink density.

A major pitfall in the studies aiming on improving the mechanical resistance of capsules is the lack of standardization of technologies to quantify the durability of capsules. Many are the disputes about laboratory variations in stability of capsules. At present most groups apply home-made procedures for quantifying mechanical resistance in which specific details such as incubation solutions, compressive force, and shaking speed are rarely documented.

One of the most commonly applied assays to quantify mechanical resistance is the osmotic pressure test in which capsules are exposed to various deleterious solutions with the aim to quantify the swelling of capsules. Swelling of the capsules leads to capsule heterogeneity and to a gradual increase in undesired capsule pore size and permeability. Different types of reagents have been used as swelling solutions including water [55], saline, citrate [56], dilutions of serum free media [65], serum [66], glycine buffer [61], and hepatozyme culture medium [67]. The advantage of this technique is that it is nonlaborious and readily available in all laboratories. However, in order to allow reproducibility it is imperative to standardize the solution reagents.

Another assay that is nowadays more commonly applied is evaluation of the physical integrity of the capsules by using a surface texture analyzer [53,68]. With this technique a specific force is placed on the capsules. The quantity of deformation or rupture of capsules is applied as a measure for the mechanical stability of the capsules. Although very reproducible the technology requires consensus about the speed of the compressive force and the extent of such compression in order to allow comparisons between laboratories. The texture analyzer can be combined by shaking the capsules by means of an orbital shaker to compare the stability between different types of microcapsules [69]. Also, there are new approaches which are not yet generally applied in the field of encapsulation. A promising approach is the probing technique to mechanically characterize small-scale structures ( $<100 \mu m$ ). This can be done by optical tweezers [70], micropipette aspiration [71], atomic force microscopy (AFM) [72], and magnetic bead measurement techniques [73]. Recently, a new force feedback microelectromechanical (MEMS) microgripper has been reported (Fig. 3). This MEMS combines the capacity to manipulate micrometer-sized biomaterials and hydrogel particles while simultaneously quantifying their mechanical properties [74]. This new MEMS microgripper integrates two-axis force feedback to protect the fragile microgripper by detecting contact between the particle and the microgripper. By that it provides gripping force feedback for achieving secure grasping without applying excessive gripping forces. Using this approach, Kim et al. [74] were the first to apply this on capsules and successfully measured Young's modulus and viscoelastic parameters of 15-25 µm-sized chitosan coated alginate microparticles. These advances may help to establish a range of predictable techniques which will provide comprehensive and comparable data without too much lab-to-lab variations about the strength of the polymer microcapsules.

## 5. Surface properties of capsules

The surface properties of capsules determine the functional performance of the capsule. It is the site that is responsible for the biocompatibility and it determines the diffusion properties. Surprisingly until a few years ago the surface of the capsule only received minor attention. This has recently changed after the introduction of new physico-chemical technologies to the field [75–80]. To illustrate the importance of the surface analysis in the field, we will discuss a few findings with alginate-based micro-capsules for encapsulation of mammalian cells.

In order to provide more insight in the structure of alginate-PLL capsules a physico-chemical analysis of the capsules has been performed by applying X-ray photoelectron spectroscopy [81]. This technique allows for identification of the chemical groups on the surface of the capsule on an atomic level. Up to now the capsule was assumed to be composed of a core of calcium-alginate which is enveloped by a membrane composed of two layers, i.e. an inner layer of alginate-PLL and an outer layer of calcium-alginate. The data, which have lead to this model, were almost exclusively obtained by studying the chemical interactions of PLL with solved, non-calcium bound and often individual components of alginate (i.e. G and M monomers) and not by studying the chemical structure of the capsules as such. In subsequent studies on true capsules, Fourier transform infrared spectroscopy, X-ray photoelectron



Fig. 3. (a) Schematic illustration of an experimental situation in which a microcapsule coated with 2% chitosan is analyzed; (b) the capsule is compressed; (c) 10% deformation of the capsule and (d) 20% deformation at 962 nN. Printed with permission from Kim K, Park H, Kwon KH, Park JY, Baek JY, Lee TS et al. A cell culturing system that integrates the cell loading function on a single platform and evaluation of the pulsatile pumping effect on cells. Biomed Microdev 2008;10:11-20.

spectroscopy (XPS), and confocal microscopy were applied to study the structure of the alginate-PLL capsule membrane [75–80]. From confocal images and from electron microscopy pictures it was visualized that the PLL penetrates the alginate core, forming an alginate-PLL complex of about 30  $\mu$ m, depending on the exposure time to PLL. It was found that the capsules were not composed of a generally considered three-layer system of alginate-polycation, and an outer alginate layer but only of an alginate-core surrounded by an alginate-polycation shell. This was recently confirmed by Tam et al. by applying ToF-SIMS imaging [80]. Fig. 4 shows the actual structure of alginate-PLL capsules.

# 6. Biocompatibility of microcapsules

The design of a standard technology for measuring biocompatibility of microcapsules is a very complex and difficult task mainly due to the complicated interactions between biological systems and microcapsules. Biocompatibility issues of microcapsules are often connected with the ability of a material to perform with an appropriate host response in a specific application [82]. For encapsulation this "specific application" is dependent on the field of application. Roughly, we can distinguish two specific applications in which optimal biocompatibility is essential. The first one is the application of encapsulation in the field of medicine and pharmacy. In this field, the capsules are applied to encapsulate cells for transplantation in recipients [83–85], and for controlled release of drugs [86–90]. The second application is the encapsulation of cells in biotechnology. Usually in this field encapsulated microbial cells are applied as biocatalysts for the production of valuable substances. Production processes are often performed under nonphysiological conditions. The cells themselves either use substances with a sequestering effect on immobilization matrices [91] or produce compounds that have inhibitory impact on cells [92]. Therefore, it is desirable to recognize and standardize proper encapsulation methods, which provide mild and physiological conditions to cells during encapsulation and post-encapsulation procedures.

Traditionally the medicine and pharmacy field were focused on the host response to the capsule materials while the biotechnology was concentrated on the compatibility of the materials with the cells in the capsules. Nowadays, it has become more and more recognized that also in the field of medicine the materials should allow adequate function of the cells in the capsules. Therefore, in the present review we discuss both the field of medicine and pharmacy and the biotechnology since it is our expectation that this will contribute to the exchange and introduction of new technologies in the different fields.

# 6.1. Biocompatibility tests in medicine and pharmacy

Biocompatibility of microcapsules in medicine and pharmacy has been the subject of intensive research, as summarized in several review articles [55,83,85,86]. Table 1 lists the most important technologies and approaches to the measurement of biocompatibility of microcapsules in the mentioned fields. Mostly the studies are dedicated to the host response against the capsule's surface. The biocompatibility was usually evaluated from multiple points of view, and assessed by a combination of techniques. The most commonly applied approach is the correlation of biological responses to capsules with their chemistry [81] and correlation of tissue reactions against capsules with the structure of the capsule's surface [75]. Many have been the efforts to identify and quantify the key markers of biocompatibility of microcapsules. However, divergence of technologies for measuring biocompatibility markers may lead to the neverending development of experimental protocols that lack standardization. Additionally, the non-consistency of biocompatibility markers can be illustrated by a number of approaches used to evaluate the same marker as shown in the first column of Table 1. The presented description of discrepancies in the biocompatibility



Fig. 4. The considered and the actual structure of alginate-PLL capsules. The capsule is not composed of three layers as generally assumed but of two layers.

evaluation of microcapsules can be considered to be an important milestone of standardization activities in the encapsulation community.

# 6.2. Biocompatibility tests in biotechnology

Basic studies of the physiological behavior of immobilized microbial cells have gained minor attention in spite of the broad application and rapid development of biotechnological processes based on immobilized cells since the early 1980s [93]. Though the range of more fundamental investigations has been limited in this field [93], research activities have resulted in the identification of key parameters regarding the physiology of immobilized microbial cells which may be considered as biocompatibility markers (Table 2). Importantly, the viability of cells in the capsules is a mutual attribute of the presented biocompatibility markers. Therefore, development and standardization of methods for rapid determination of viable (active) biomass are necessary in order to fully understand the physiology of microbial cells in the immobilized state, and to finetune a given biosystem. It has been shown that bioluminometry is a useful tool for determining the concentration of viable microbial cells encapsulated or entrapped in different matrices [92,94,95]. Since this technology is expected to play a major role in measuring biocompatibility of microbial cells, it will be explained in more detail below. An additional reason is that we also expect that this technology will be applied to the medicine and pharmacy field to quantify the survival of cells in immobilizing matrices.

## 6.3. Bioluminometry for determining biocompatibility properties

Viable biomass measurements are often complicated by the fact that some immobilization materials (e.g. hydrogels and polymers) may be rather difficult to dissolve in order to facilitate the biomass release followed by a gravimetric assay. Additionally, the results of typical gravimetric methods do not reflect the amount of active (viable) biomass present in the sample, and non-biocompatible immobilization materials can negatively affect the viability of cells over time. Bioluminometry offers the ability to determine the active biomass content by measuring the ATP concentration extracted from cells immobilized in hydrogel beads [94,95] and polyelectrolyte complex microcapsules [92]. Because ATP is rapidly degraded after cell death, its concentration is a good indicator of the cell viability and can be used to determine the concentration of the active biomass. The released ATP reacts with luciferin (LH<sub>2</sub>) in a reaction catalyzed by luciferase, accompanied by the emission of bioluminescent light:

$$ATP + LH_2 + \frac{1}{2}O_2 \xrightarrow{\text{fuclue ase}} LAMP + P - P + H_2O + hv$$

The efficient extraction of intracellular ATP is possible mainly due to the fact that 90% of the active biomass is located in a 140- $\mu$ m thick outer layer of gel beads [96], which allows for easy release and diffusion of ATP out of the immobilized cells (Fig. 5a). Subsequent addition of the ATP monitoring reagent is followed by measuring the bioluminescence response (Fig. 5b). The light output expressed as RLU (relative light units) corresponds to the concentration of active biomass in the beads. The comparison shown in Fig. 3c exhibits a high degree of correlation ( $r^2 = 0.9998$ ), making the bioluminometric method a rapid and accurate alternative to the well-established gravimetric assay.

## 7. Storage conditions for microcapsules

Storage of encapsulated cells for transport or in the time period between manufactory and application is mandatory for almost all fields of encapsulation. Determination of suitable conditions for 2566

#### Table 1

The most common technologies for measuring biocompatibility properties of microcapsules in biomedicine and pharmacy.

Biocompatibility marker	Technologies of measurement	References
Pericapsular cell overgrowth		
Score of cell overgrowth	Light microscopy evaluation	[76,87,89,114–119]
Fibrosis score	Analysis of digitized images	[119–121]
Percentage of clean capsules	Cell adhering test	[122]
Area of capsular fibrosis	Histological analysis	[81,88–90,115,120,123–131]
Percentage of capsular overgrowth	Immunohistochemical evaluation	[114,116]
Degree of capsular overgrowth	SEM <sup>a</sup> analysis	[90,118]
Frequency of overgrowth	Fluorophotometry	[129,132]
Cellular composition of overgrowth	Liquid scintillation counting	[129,132]
Cell adhering ratio		
DNA content		
Glucose oxidation rate		
Viability of encapsulated cells		
Cell vitality	Fluorescent live/dead staining by CLSM <sup>b</sup>	[120]
Cell viability		
In-bead survival rate		[130]
Proliferation of cells	Life-Dead-Assay examined by fluorescent microscopy	[65]
Cellular mortality		
Cell death	Alamar Blue assay by fluorometry	[123,131]
	Propidium iodide staining	[133]
	MIT <sup>e</sup> assay	[133–136]
	Trypan blue exclusion assay	[130]
	Optical density measurement	[131,136]
Response of implantation site to microcaps	ules	
Inflammation at the implantation site	MTS <sup>d</sup> colorimetric assay	[87,131]
Tissue damage	Optical microscopy evaluation	[137]
Pro-inflammatory response	Quantitative autoradiography	[138]
Immune/immunological response	Quantification of tumor necrosis factor alpha	[126]
Immunoreactions	Mitogenic activity assay	[75,88,90,127,130]
Host reaction to microcapsules	Histological analysis	[139]
Tissue reactions/responses	Absorbance to detect antibodies in serum	[134,140]
	RT-PCR <sup>e</sup> measurement of cytokine mRNA expression in macrophages	[65,76,81,116,117,120,127–129,132]
Recovery rate of microcansules		
Retrieval/recovery rate	Volumetry	[138]
Microcapsule recovery	Toxilight assay	[135]
Cytotoxicity	Measurement of lactate dehydrogenase activity	[136]
	MTS colorimetric assav	[-30]
Floating cells in peritoneal cavity	Hemocytometry	[115]
Secretion of proteins	Bradford dve-binding procedure	[135]

<sup>a</sup> Scanning electron microscopy.

<sup>b</sup> Confocal laser scanning microscopy.

<sup>c</sup> 3-(4,5-Dimethyl-2-yl)-2,5-diphenyltetrazolium bromide.

<sup>d</sup> 3-(4,5-Dimethylthiazol-2-yl)-5-(3-carboxymethoxyphenyl)-2H-tetrazolium, inner salt.

<sup>e</sup> Semiquantitative reverse transcriptase-polymerase chain reaction.

storage of microcapsules, however, plays an underestimated role in microencapsulation research. This is rather surprising since it is broadly accepted that microcapsule characteristics and functionality are often very sensitive to environmental parameters such as temperature, humidity, osmotic pressure, storage solution, or solvent [97–100]. In this review we have decided to separately discuss storage requirements since it is predictable that the large variations in outcome of encapsulation systems can partly be attributed to differences in storage of the encapsulated cells before application. It is mandatory to choose the storage conditions as such that it ensures maintenance of optimal performance.

The adequacy of a storage condition depends on the field of application and on which capsule characteristic should be maintained. It also involves the measurement of characteristics over time preferably focused on the variation of only one environmental parameter such as type of storage solution or temperature. Thereby, analysis can focus on changes in physical or chemical microcapsule properties such as diffusivity, mechanical strength or swelling [101–103], or on changes in properties of encapsulated cells such as catalytic activity [104,105], or performance as analyst. Time course, choice of parameter, and focus of the investigation strongly depend on the exact composition and application of the microcapsules.

For characterization of changes in essential physical and chemical microcapsule characteristics many techniques as already described in the previous sections of this article can be applied. It is essential to monitor the microstructures of capsules. Commonly applied technologies up to now are phase transition, retention. Integrity is usually assessed by imaging techniques such as optical microscopy, scanning electron microscopy (SEM), electron spin resonance spectroscopy (ESR), nuclear magnetic resonance spectroscopy (NMR), radioactive tracers, or fluorescence quenching [101], respectively. An indirect, but particularly realistic measure with regard to application comprises the determination of rupture time by an in situ observation of the release of active compounds such as drugs from microcapsule carriers [102,106]. Such an investigation requires a rather different set of analytical methods involving standard techniques for analysis of structure and concentration of dissolved compounds, such as NMR, mass spectrometry, GC, or HPLC. These are also useful for the determination of changes in properties of the encapsulated material. If functionality of this material mainly depends on chemical stability, as for drugs, cosmetics, or food ingredients [100], complete extraction of the active compounds from the microcapsules must usually precede the measurement [107-109], as methods for direct quantification of

#### Table 2

The most common technologies for measuring biocompatibility properties of microcapsules and beads in biotechnology.

Biocompatibility marker	Technologies of measurement	References
Viability of immobilized cells	Bioluminometry and gravimetry Sample staining with Live/Dead BacLight viability kit examined by epifluorescence microscopy and CLSM Viable cell counting Determination of CFU <sup>a</sup> Radiometry for measurement of protein and nucleic acid synthesis through <sup>14</sup> C amino acids and <sup>14</sup> C nucleic acids incorporated into cell proteins and DNA	[91,94,95] [136] [141,142] [143,144] [143]
Growth rate of immobilized cells	Optical density measurement Chlorophyll absorbance assay Counting of cells by hemocytometry Colony counting on agar plates On-line microscopy analysis Assessment of dry cell weight Cell protein content by Lowry method <sup>31</sup> P and <sup>13</sup> C NMR studies	[141,145,146] [147] [148] [142,149,150] [151] [150,152] [150] [153]
Biocatalytic efficiency and enzyme expression of immobilized cells	HPLC analysis Estimation of enzymatic activity by spectrophotometry Measurement of induced leakage of UV-absorbing substances from immobilized cells by spectrophotometry	[154,155] [142,145,156] [157]
Stress resistance of immobilized cells	Scintillation counting and ion release Spectrophotometry	[158] [159]
Variations in protein spot densities observed on protein maps Plasmid stability of immobilized recombinant cells Respiratory activity	Principal component analysis of spot quantity variations on electrophoretogram obtained by 2-D electrophoresis Screening of cell colonies for antibiotic resistance by culturing on agar plates $^{14}CO_2$ measurement	[149,160] [161–164] [143]

<sup>a</sup> Colony-forming units.

chemical compounds within capsules are still rare. In contrast, performance of catalytically active compounds, like whole cell biocatalysts or enzymes, is usually approached while the catalysts remain in the capsules. The activity is then monitored via the reaction kinetics which can either be derived from the concentration of reactants allowed to diffuse in and out of the capsules [105,110], or more elegantly from the heat release during reaction. The latter uses flow calorimetry (FC) as a thermal biosensor, and has been successfully applied to the characterization of various types of encapsulated biocatalysts [111–113].

# 8. Concluding remarks

In spite of the tremendous growth of the industrial and clinical application of encapsulation in the past decade, it is still difficult if not impossible to define the requirement capsules have to meet in order to provide long-term functionality of the enveloped cells or bioactive components. For a further development of the technology and an exchange of technologies it is mandatory to standardize and define technologies that measure specific characteristics. The present review is the direct results of a common effort of



Fig. 5. Measurement of the active biomass concentration in hydrogels. (a) 90% of the active biomass is located in a 140-µm layer of a gel bead. (b) Upon addition of ATP release buffer and ATP monitoring reagent to immobilized cells, bioluminometric response to proportional to the intracellular ATP content is generated and detected. (c) Comparison of the biomass concentration as determined by the luminometric (Y-axis) and gravimetric (X-axis) methods. All data points represent an average of at least 5 consecutive measurements.

researchers combined in the COST865 – action to define standardized protocols for characterization and standardization of microcapsule properties for a given application. The studies involve not only inventarisation and comparison of technologies on the basis of own experiences and published results but also on the basis of exchange of capsules and technologies in order to understand lab-to-lab variations and identification of technical details that require further standardization. The efforts are summarized on http://impascience.eu/COST865/index101.html.

Up to now five types of characterizations have been identified as mandatory for adequate description of a capsule. These are the characterization of the polymers applied, the permeability, the surface properties, the biocompatibility, but also the storage conditions. All these factors have a mutual influence on the functional properties of the final capsule.

Obviously, the authors are aware that the identification of mandatory characterizations will not immediately lead to a full implication of this assessment in studies in the near future. The application requires a multidisciplinary approach in which biomedical, physical, and chemical technologies are combined. However, for adequate reproducibility and for understanding variations in outcome of capsules it is advisable if not mandatory to include the characterization in future studies. The described technologies in the present review may be helpful in accomplishing these goals.

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#### References

- Bodeutsch T, James EA, Lee JM. The effect of immobilization on recombinant protein production in plant cell culture. Plant Cell Rep 2001;20:562–6.
- [2] Dornenburg H. Evaluation of immobilisation effects on metabolic activities and productivity in plant cell processes. Proc Biochem 2004;39:1369–75.
  [3] Shibli RA, Al Ababneh SS, Smith MAL. Cryopreservation of plant germplasm.
- Dirasat Agric Sci 2004;31:60–73. [4] Shah NP. Probiotic bacteria: selective enumeration and survival in dairy
- foods. J Dairy Sci 2000;83:894–907. [5] Chattopadhyaya S, Singhal RSA, Kulkarni PR. Oxidized starch as gum Arabic
- substitute for encapsulation of flavours. Carbohydr Polym 1998;37:143–4. [6] O'Reilly AM, Scott JA. Defined coimmobilization of mixed microorganism
- [6] O Kenny AM, Scott JA. Defined commonization of mixed microorganism cultures. Enzyme Microb Technol 1995;17:636–46.
- [7] Doleyres Y, Lacroix C. Technologies with free and immobilised cells for probiotic bifidobacteria production and protection. Int Dairy J 2005;15: 973–88.
- [8] Muthukumarasamy P, Holley RA. Survival of *Escherichia coli* O157: H7 in dry fermented sausages containing micro-encapsulated probiotic lactic acid bacteria. Food Microbiol 2007;24:82–8.
- [9] Anjani K, Iyer C, Kailasapathy K. Survival of co-encapsulated complementary probiotics and prebiotics in yoghurt. Milchwissenschaft 2004;59:396–9.
- [10] Iyer C, Kailasapathy K. Effect of co-encapsulation of probiotics with prebiotics on increasing the viability of encapsulated bacteria under in vitro acidic and bile salt conditions and in yogurt. J Food Sci 2005;70:M18–23.
- [11] Sultana K, Godward G, Reynolds N, Arumugaswamy R, Peiris P, Kailasapathy K. Encapsulation of probiotic bacteria with alginate-starch and evaluation of survival in simulated gastrointestinal conditions and in yoghurt. Int J Food Microbiol 2000;62:47–55.
- [12] Guerin D, Vuillemard JC, Subirade M. Protection of bifidobacteria encapsulated in polysaccharide-protein gel beads against gastric juice and bile. J Food Prot 2003;66:2076–84.
- [13] Urbanska AM, Bhathena J, Prakash S. Live encapsulated *Lactobacillus acido-philus* cells in yogurt for therapeutic oral delivery: preparation and in vitro analysis of alginate-chitosan microcapsules. Can J Physiol Pharmacol 2007;85:884–93.
- [14] Champagne CP, Fustier P. Microencapsulation for the improved delivery of bioactive compounds into foods. Curr Opin Biotechnol 2007;18:184–90.
- [15] De Vos P, Faas MM, Strand B, Calafiore R. Alginate-based microcapsules for immunoisolation of pancreatic islets. Biomaterials 2006;27:5603–17.
- [16] Zimmermann H, Zimmermann D, Reuss R, Feilen PJ, Manz B, Katsen A, et al. Towards a medically approved technology for alginate-based microcapsules allowing long-term immunoisolated transplantation. J Mater Sci Mater Med 2005;16:491-501.

- [17] Koo J, Chang TSM. Secretion of erythropoietin from microencapsulated rat kidney cells. Int J Artif Organs 1993;16:557-60.
- [18] Chang PL, Shen N, Westcott AJ. Delivery of recombinant gene products with microencapsulated cells in vivo. Hum Gene Ther 1993;4:433-40.
- [19] Liu HW, Ofosu FA, Chang PL. Expression of human factor IX by microencapsulated recombinant fibroblasts. Hum Gene Ther 1993;4:291–301.
- [20] Cieslinski DA, Humes HD. Tissue engineering of a bioartificial kidney. Biotechnol Bioeng 1994;43:678–81.
- [21] Wong H, Chang TM. Bioartificial liver: implanted artificial cells microencapsulated living hepatocytes increases survival of liver failure rats. Int J Artif Organs 1986;9:335–6.
- [22] Aebischer P, Russell PC, Christenson L, Panol G, Monchik JM, Galletti PM. A bioartificial parathyroid. ASAIO Trans 1986;32:134–7.
- [23] Aebischer P, Goddard M, Signore AP, Timpson RL. Functional recovery in hemiparkinsonian primates transplanted with polymer-encapsulated PC12 cells. Exp Neurol 1994;126:151–8.
- [24] Lim F, Sun AM. Microencapsulated islets as bioartificial endocrine pancreas. Science 1980;210:908-10.
- [25] Calafiore R, Basta G, Luca G, Lemmi A, Montanucci MP, Calabrese G, et al. Microencapsulated pancreatic islet allografts into nonimmunosuppressed patients with type 1 diabetes: first two cases. Diabetes Care 2006;29:137–8.
- [26] Grasdalen H. High-field, <sup>1</sup>H-NMR spectroscopy of alginate: sequential study and linkage conformations. Carbohydr Res 1983:225–60.
- [27] Grasdalen H, Larsen B, Smidsrod O. A P.M.R. study of the composition and sequence of uronate residues in alginates. Carbohydr Res 1979:23–31.
  [28] Grasdalen H, Larsen B, Smidsrod O. <sup>13</sup>C-NMR studies of monomeric compo-
- [28] Grasdalen H, Larsen B, Smidsrod O. '2C-NMR studies of monomeric composition and sequence in alginate. Carbohydr Res 2008:179–91.
- [29] Zimmermann U, Klöck G, Federlin K, Hannig K, Kowalski M, Bretzel RG, et al. Production of mitogen-contamination free alginates with variable ratios of mannuronic acid to guluronic acid by free flow electrophoresis. Electrophoresis 1992;13:269–74.
- [30] De Vos P, De Haan BJ, Wolters GHJ, Strubbe JH, Van Schilfgaarde R. Improved biocompatibility but limited graft survival after purification of alginate for microencapsulation of pancreatic islets. Diabetologia 1997;40:262–70.
- [31] Montaudo G, Samperi F, Montaudo MS. Characterization of synthetic polymers by MALDI-MS. Progr Polym Sci 2006;31:277–357.
- [32] Schnoll-Bitai I, Ullmer R, Hrebicek T, Rizzi A, Lacik I. Characterization of the molecular mass distribution of pullulans by matrix-assisted laser desorption/ionization time-of-flight mass spectrometry using 2,5-dihydroxybenzoic acid butylamine (DHBB) as liquid matrix. Rapid Commun Mass Spectrom 2008;22:2961–70.
- [33] Lacík I. Polymer chemistry in diabetes treatment by encapsulated islets of Langerhans: review to 2006. Aust J Chem 2006;59:508–24.
- [34] Muhr AH, Blanshard JMV. Diffusion in gels. Polymer 1982;23:1012-26.
- [35] Marsich E, Borgogna M, Donati I, Mozetic P, Strand BL, Salvador SG, et al. Alginate/lactose-modified chitosan hydrogels: a bioactive biomaterial for chondrocyte encapsulation. J Biomed Mater Res 2008;84:364–76.
- [36] Schuldt U, Hunkeler D. Characterization methods for microcapsules. Minerva Biotechnologica 2000;12:249–64.
- [37] Uludag H, de-Vos P, Tresco PA. Technology of mammalian cell encapsulation. Adv Drug Deliv Rev 2000;42:29–64.
- [38] Kulseng B, Thu B, Espevik T, Skjåk-Bræk G. Alginate polylysine microcapsules as immune barrier: permeability of cytokines and immunoglobulins over the capsule membrane. Cell Transplant 1997;6:387–94.
- [39] Morch YA, Donati I, Strand BL, Skjåk-Bræk G. Effect of Ca, Ba and Sr on alginate microbeads. Biomacromolecules 2006;7:1471–80.
- [40] Brissova M, Lacik I, Powers AC, Anilkumar AV, Wang T. Control and measurement of permeability for design of microcapsule cell delivery system. J Biomed Mater Res 1998;39:61–70.
- [41] Brissova M, Petro M, Lacik I, Powers AC, Wang T. Evaluation of microcapsule permeability via inverse size exclusion chromatography. Anal Biochem 1996;242:104–11.
- [42] Lewinska D, Rosinski S, Hunkeler D, Poncelet D, Werynski A. Mass transfer coefficient in characterization of gel beads and microcapsules. J Memb Sci 2002;209:533–40.
- [43] Chen G, Yao SJ, Guan YX, Lin DQ. Preparation and characterization of NaCS-CMC/PDMDAAC capsules. Colloids Surf B Biointerfaces 2005;45:136–43.
- [44] Stefuca V, Gemeiner P, Kurillova L, Dautzenberg H, Polakovic M, Bales V. Polyelectrolyte complex capsules as a material for enzyme immobilization. Catalytic properties of encapsulated lactate dehydrogenase. Appl Biochem Biotechnol 1991;30:313–24.
- [45] Young THRA, Chuang WY, Yao NK, Chen LW. Use of a diffusion model for assessing the performance of poly(vinyl alcohol) bioartificial pancreases. J Biomed Mater Res 1998;40:385–91.
- [46] Martinsen A, Storro I, Skjåk-Bræk G. Alginate as immobilization material III. Diffusional properties. Biotechnol Bioeng 1992;39:186–94.
- [47] Shin HS, Kim YS, Lee YM, Lee KH, Kim SJ, Rogers CE. Electrochemical behavior of an interpenetrating polymer network hydrogel composed of poly(propylene glycol) and poly(acrylic acid). J Appl Polym Science 1998;89:2301–5.
- [48] Desai TA. Microfabrication technology for pancreatic cell encapsulation. Expert Opin Biol Ther 2002;2:633–46.
- [49] Desai TA, West T, Cohen M, Boiarski T, Rampersaud A. Nanoporous microsystems for islet cell replacement. Adv Drug Deliv Rev 2004;56:1661–73.
- [50] La Flamme KE, Popat KC, Leoni L, Markiewicz E, La Tempa TJ, Roman BB, et al. Biocompatibility of nanoporous alumina membranes for immunoisolation. Biomaterials 2007;28:2638–45.

- [51] La Flamme KE, Mor G, Gong D, La Tempa T, Fusaro VA, Grimes CA, et al. Nanoporous alumina capsules for cellular macroencapsulation: transport and biocompatibility. Diabetes Technol Ther 2005;7:684–94.
- [52] Chang TM. Therapeutic applications of polymeric artificial cells. Nat Rev Drug Discov 2005;4:221–35.
- [53] Thanos CG, Bintz BE, Emerich DF. Stability of alginate-polyornithine microcapsules is profoundly dependent on the site of transplantation. J Biomed Mater Res A 2007;81:1-11.
- [54] Chia SM, Wan AC, Quek CH, Mao HQ, Xu X, Shen L, et al. Multi-layered microcapsules for cell encapsulation. Biomaterials 2002;23:849–56.
- [55] Darrabie MD, Kendall WFJ, Opara EC. Characteristics of poly-L-ornithinecoated alginate microcapsules. Biomaterials 2005;26:6846–52.
- [56] Orive G, Hernandez RM, Gascon AR, Igartua M, Pedraz JL. Development and optimisation of alginate-PMCG-alginate microcapsules for cell immobilisation. Int J Pharm 2003;259:57–68.
- [57] Thu B, Bruheim P, Espevik T, Smidrod O, Soon-Shiong P, Skjak-Braek G. Alginate polycation microcapsules. I. Interaction between alginate and polycation. Biomaterials 1996;17:1031–40.
- [58] Smidsrod O, Skjak-Break G. Alginate as immobilization matrix for cells. Trends Biotechnol 1990;8:71–8.
- [59] Strand BL, Morch YA, Syvertsen KR, Espevik T, Skjak-Braek G. Microcapsules made by enzymatically tailored alginate. | Biomed Mater Res A 2003;64:540–50.
- [60] Cellesi F, Tirelli N, Hubbell JA. Towards a fully-synthetic substitute of alginate: development of a new process using thermal gelation and chemical cross-linking. Biomaterials 2004;25:5115–24.
- [61] Dusseault J, Leblond FA, Robitaille R, Jourdan G, Tessier J, Menard M, et al. Microencapsulation of living cells in semi-permeable membranes with covalently cross-linked layers. Biomaterials 2005;26:1515–22.
- [62] Rokstad AM, Donati I, Borgogna M, Oberholzer J, Strand BL, Espevik T, et al. Cell-compatible covalently reinforced beads obtained from a chemoenzymatically engineered alginate. Biomaterials 2006;27:4726–37.
- [63] Schmidt JJ, Rowley J, Kong HJ. Hydrogels used for cell-based drug delivery. J Biomed Mater Res 2008;87:1113–22.
- [64] Weeks TS, Adolf D, McCoy JD. Cohesive failure in partially cured epoxies. Macromolecules 1999;32:1918–22.
- [65] Shen F, Li AA, Cornelius RM, Cirone P, Childs RF, Brash JL, et al. Biological properties of photocrosslinked alginate microcapsules. J Biomed Mater Res 2005;75B:425–34.
- [66] De Castro M, Orive G, Hernandez RM, Gascon AR, Pedraz JL. Comparative study of microcapsules elaborated with three polycations (PLL, PDL, PLO) for cell immobilization. J Microencapsul 2005;22:303–15.
- [67] Yin C, Chia SM, Quek CH, Yu H, Zhuo RX, Leong KW, et al. Microcapsules with improved mechanical stability for hepatocyte culture. Biomaterials 2003;24:1771–80.
- [68] Rosinski S, Grigorescu G, Lewinska D, Ritzen LG, Viernstein H, Teunou E, et al. Characterization of microcapsules: recommended methods based on roundrobin testing. J Microencapsul 2002;19:641–59.
- [69] Leblond FA, Tessier J, Halle JP. Quantitative method for the evaluation of biomicrocapsule resistance to mechanical stress. Biomaterials 1996;17: 2097–102.
- [70] Fontes A, Fernandes HP, de Thomaz AA, Barbosa LC, Barjas-Castro ML, Cesar CL. Measuring electrical and mechanical properties of red blood cells with double optical tweezers. J Biomed Opt 2008;13:014001.
- [71] Hochmuth RM. Micropipette aspiration of living cells. J Biomech 2000;33:15–22.
- [72] Dulinska I, Targosz M, Strojny W, Lekka M, Czuba P, Balwierz W, et al. Stiffness of normal and pathological erythrocytes studied by means of atomic force microscopy. J Biochem Biophys Methods 2006;66:1–11.
- [73] Bausch AR, Moller W, Sackmann E. Measurement of local viscoelasticity and forces in living cells by magnetic tweezers. Biophys J 1999;76:573–9.
- [74] Kim K, Liu X, Zhang Y, Cheng J, Yu WX, Sun Y. Elastic and viscoelastic characterization of microcapsules for drug delivery using a force-feedback MEMS microgripper. Biomed Microdevices 2008.
- [75] Bunger CM, Gerlach C, Freier T, Schmitz KP, Pilz M, Werner C, et al. Biocompatibility and surface structure of chemically modified immunoisolating alginate-PLL capsules. J Biomed Mater Res 2003;67A:1219–27.
- [76] De Vos P, Van Hoogmoed CG, van Zanten J, Netter S, Strubbe JH, Busscher HJ. Long-term biocompatibility, chemistry, and function of microencapsulated pancreatic islets. Biomaterials 2003;24:305–12.
- [77] De Vos P, Andersson A, Tam SK, Faas MM, Halle JP. Advances and barriers in mammalian cell encapsulation for treatment of Diabetes. Immun Endoc Metab Agents Med Chem 2006:139–53.
- [78] De Vos P, De Haan BJ, Kamps JA, Faas MM, Kitano T. Zeta-potentials of alginate-PLL capsules: a predictive measure for biocompatibility? J Biomed Mater Res 2007;80:813–9.
- [79] Van Hoogmoed CG, Busscher HJ, De Vos P. Fourier transform infrared spectroscopy studies of alginate-PLL capsules with varying compositions. J Biomed Mater Res 2003;67A:172–8.
- [80] Tam SK, Dusseault J, Polizu S, Menard M, Halle JP, Yahia L. Physicochemical model of alginate-poly-u-lysine microcapsules defined at the micrometric/ nanometric scale using ATR-FTIR, XPS, and ToF-SIMS. Biomaterials 2005;26:6950–61.
- [81] De Vos P, Van Hoogmoed CG, Busscher HJ. Chemistry and biocompatibility of alginate-PLL capsules for immunoprotection of mammalian cells. J Biomed Mater Res 2002;60:252–9.

- [82] Williams DF. Summary and definitions. In: Progress in biomedical engineering: definition in biomaterials (4). Amsterdam: Elsevier Science Publisher BV; 1987. p. 66–71.
- [83] Mikos AG, Papadaki MG, Kouvroukoglou S, Ishaug SL, Thomson RC. Minireview: Islet transplantation to create a bioartificial pancreas. Biotechnol Bioeng 1994;43:673–7.
- [84] De Vos P, Faas MM, Strand B, Calafiore R. Alginate-based microcapsules for immunoisolation of pancreatic islets. Biomaterials 2006;27:5603–17.
- [85] De Vos P, Tatarkiewicz K. Considerations for successful transplantation of encapsulated pancreatic islets. Diabetologia 2002;45:159–73.
- [86] Fournier EA, Passirani C, Montero Menei CN, Benoit JP. Biocompatibility of implantable synthetic polymeric drug carriers: focus on brain biocompatibility. Biomaterials 2003;24:3311–31.
- [87] Ricci M, Blasi P, Giovagnoli S, Rossi C, Macchiarulo G, Luca G, et al. Ketoprofen controlled release from composite microcapsules for cell encapsulation: effect on post-transplant acute inflammation. J Control Release 2005;107:395–407.
- [88] Reithmeier H, Herrmann J, Goepferich A. Lipid microparticles as a parenteral controlled release device for peptides. J Control Release 2001;73:339–50.
- [89] Blasi P, Giovagnoli S, Schoubben A, Ricci M, Rossi C, Luca G, et al. Preparation and in vitro and in vivo characterization of composite microcapsules for cell encapsulation. Int J Pharm 2006;324:27–36.
- [90] Blanco MD, Bernardo MV, Sastre RL, Olmo R, Muniz EA, Teijon JM. Preparation of bupivacaine-loaded poly(epsilon-caprolactone) microspheres by spray drying: drug release studies and biocompatibility. Eur J Pharm Biopharm 2003;55:229–36.
- [91] Bucko M, Vikartovska A, Lacik I, Kollarikova G, Gemeiner P, Patoprsty V, et al. Immobilization of a whole-cell epoxide-hydrolyzing biocatalyst in sodium alginate-cellulose sulfate-poly(methylene-co-guanidine) capsules using a controlled encapsulation process. Enzyme Microb Technol 2005;36:118–26.
- [92] Stark D, Kornmann H, Munch T, Sonnleitner B, Marison IW, von Stockar U. Novel type of in situ extraction: use of solvent containing microcapsules for the bioconversion of 2-phenylethanol from L-phenylalanine by Saccharomyces cerevisiae. Biotechnol Bioeng 2003;83:376–85.
- [93] Junter GA, Jouenne T. Immobilized viable microbial cells: from the process to the proteome em leader or the cart before the horse. Biotechnol Adv 2004;22:633–58.
- [94] Navratil M, Domeny Z, Hronsky V, Sturdik E, Smogrovicova D, Gemeiner P. Use of bioluminometry for determination of active yeast biomass immobilized in ionotropic hydrogels. Anal Biochem 2000;284:394–400.
- [95] Navratil M, Svitel J, Gemeiner P. Bioluminescence in immobilized cells for biomass detection and biosensor applications. In: Guisan JM, editor. Methods in biotechnology. Immobilization of enzymes and cells. Totowa, NJ: Humana Press; 2006. p. 393–401.
- [96] Zaghloul TI, Hendawy HM, El Assar SA, Mostafa MH. Enhanced stability of the cloned *Bacillus subtilis* alkaline protease gene in alginate-immobilized *B. subtilis* cells. Enzyme Microb Technol 2002;30:862–6.
- [97] Gibbs BF, Kermasha S, Alli I, Muligan C, Anon A. Constant air quality humidity and temperature control during soft capsule manufacturing. Chemical Plants Processing 2002;1:22–3.
- [98] Vinogradova OI. Mechanical properties of polyelectrolyte multilayer microcapsules. J Physiol 2004;16:32–6.
- [99] Gupta V, Verma S, Nanda A, Nanda S. Osmotically controlled drug delivery. Drug Del Technol 2005;5:68–76.
- [100] Pirvu C. Chemical characterization and applications of microcapsules. Farmacia 2005;53:61–8.
- [101] Shaidi F, Han XQ. Encapsulation of food ingredients. Crit Rev Food Sci Nutr 1993;33:501–47.
- [102] Recio R, Bassol S. Effects of storage and temperature upon soft jelly capsules containing nonoxynol as spermicide. Contraception 1995;51:201–2.
- [103] Doumeche B, Kuppers M, Stapf S, Blumich B, Hartmeier W, Ansorge-Schumacher MB. New approaches to the visualization, quantification and explanation of acid-induced water loss from Ca-alginate hydrogel beads. J Microencapsul 2004;21:565–73.
- [104] Kurillova L, Gemeiner P, Ilavsky M, Stefuca V, Polakovic M, Welwardova A, et al. Calcium pectate gel beads for cell entrapment: 4. Properties of stabilized and hardened calcium pectate gel beads with and without cells. Biotechnol Appl Biochem 1992;16:236–51.
- [105] De Temino DMR, Hartmeier W, Ansorge Schumacher MB. Entrapment of the alcohol dehydrogenase from *Lactobacillus kefir* in polyvinyl alcohol for the synthesis of chiral hydrophobic alcohols in organic solvents. Enzyme Microb Technol 2005;36:3–9.
- [106] Johnson BF, McAuley PV, Smith PM, French JAC. The effects of storage upon in vitro and in vivo characteristics of soft gelatine capsules containing digoxin. J Pharm Pharmacol 1977;29:576–8.
- [107] de Koning AJ, Milkovich S. The storage behaviour of a number of fish oil health capsules at ambient temperature. J Food Sci 1989;1:7–8.
- [108] Lin SY, Sheen LY, Tsai TJ. Changes of microencapsulated garlic and ginger essential oils after storage. Zongguo Nongye Huaxue Huizhi 1992;30:544–52.
- [109] Ofner III CM, Zhang YE, Jobeck VC, Bowman BJ. Crosslinking studies in gelatin capsules treated with formaldehyde and in capsules exposed to elevated temperature and humidity. J Pharm Sci 2001;90:79–88.
- [110] Nguyen XT. Stability and properties of papain contained in capsules as a function of duration of storage. Tap Chi Duoc Hoc 1997;7:12–7.
- [111] Stefuca V, Gemeiner P, Kurillova L, Danielsson B, Bales V. Application of the enzyme thermistor to the direct estimation of intrinsic kinetics using the

saccharose-immobilized invertase system. Enzyme Microb Technol 1990;12:830–5.

- [112] Gemeiner P, Stefuca V, Welwardova A, Michalkova E, Welward L, Kurillova L, et al. Direct determination of the cephalosporin transforming activity of immobilized cells with use of an enzyme thermistor. 1. Verification of the mathematical model. Enzyme Microb Technol 1993;15:50–6.
- [113] Stefuca V, Gemeiner P. Investigation of catalytic properties of immobilized enzymes and cells by flow microcalorimetry. In: Scheper T, editor. Advances in biochemical engineering/biotechnology. Berlin–Heidelberg: Springer Verlag; 1999. p. 69–99.
- [114] Wilson JT, Cui W, Sun XL, Tucker Burden C, Weber CJ, Chaikof EL. In vivo biocompatibility and stability of a substrate-supported polymerizable membrane-mimetic film. Biomaterials 2007;28:609–17.
- [115] Sakai S, Mu C, Kawabata K, Hashimoto I, Kawakami K. Biocompatibility of subsieve-size capsules versus conventional-size microcapsules. J Biomed Mater Res 2006;78A:394–8.
- [116] Dufrane D, Steenberghe M, Goebbels RM, Saliez A, Guiot Y, Gianello P. The influence of implantation site on the biocompatibility and survival of alginate encapsulated pig islets in rats. Biomaterials 2006;27:3201–8.
- [117] De Vos P, De Haan B, Van Schilfgaarde R. Effect of the alginate composition on the biocompatibility of alginate-polylysine microcapsules. Biomaterials 1997;18:273–8.
- [118] Chen JP, Chu IM, Shiao MY, Hsu BR, Fu SH. Microencapsulation of islets in PEG-amine modified alginate-poly(L-lysine)-alginate microcapsules for constructing bioartificial pancreas. J Ferm Bioeng 1998;86:185–90.
- [119] Schneider S, Feilen PJ, Slotty V, Kampfner D, Preuss S, Berger S, et al. Multilayer capsules: a promising microencapsulation system for transplantation of pancreatic islets. Biomaterials 2001;22:1961–70.
- [120] Risbud MV, Bhargava S, Bhonde RR. In vivo biocompatibility evaluation of cellulose macrocapsules for islet immunoisolation: implications of low molecular weight cut-off. J Biomed Mater Res 2003;66:86–92.
- [121] Zhang H, Sun L, Wang W, Ma X. Quantitative analysis of fibrosis formation on the microcapsule surface with the use of picro-sirius red staining, polarized light microscopy, and digital image analysis. J Biomed Mater Res 2006;76A:120–5.
- [122] Chang SJ, Lee CH, Hsu CY, Wang YJ. Biocompatible microcapsules with enhanced mechanical strength. J Biomed Mater Res 2002;59:118–26.
- [123] Jork A, Thurmer F, Cramer H, Zimmermann G, Gessner P, Hamel K, et al. Biocompatible alginate from freshly collected *Laminaria pallida* for implantation. Appl Microbiol Biotechnol 2000;53:224–9.
- [124] Robitaille R, Leblond FA, Bourgeois Y, Henley N, Loignon M, Halle JP. Studies on small (<350 microm) alginate-poly-L-lysine microcapsules. V. Determination of carbohydrate and protein permeation through microcapsules by reverse-size exclusion chromatography. J Biomed Mater Res 2000;50:420–7.
- [125] Ponce S, Orive G, Gascon AR, Hernandez RM, Pedraz JL. Microcapsules prepared with different biomaterials to immobilize GDNF secreting 3T3 fibroblasts. Int J Pharm 2005;293:1–10.
- [126] Klöck G, Pfeffermann A, Ryser C, Grohn P, Kuttler B, Hahn HJ, et al. Biocompatibility of mannuronic acid-rich alginates. Biomaterials 1997;18:707–13.
- [127] Ponce S, Orive G, Hernandez R, Gascon AR, Pedraz JL, De Haan BJ, et al. Chemistry and the biological response against immunoisolating alginatepolycation capsules of different composition. Biomaterials 2006;27:4831–9.
- [128] Sawhney AS, Pathak CP, Hubbell JA. Interfacial photopolymerization of poly(ethylene glycol)-based hydrogels upon alginate-poly(l-lysine) microcapsules for enhanced biocompatibility. Biomaterials 1993;14:1008–16.
- [129] King A, Sandler S, Andersson A. The effect of host factors and capsule composition on the cellular overgrowth on implanted alginate capsules. J Biomed Mater Res 2001;57:374–83.
- [130] Bunger CM, Tiefenbach B, Jahnke A, Gerlach C, Freier T, Schmitz KP, et al. Deletion of the tissue response against alginate-pll capsules by temporary release of co-encapsulated steroids. Biomaterials 2005;26:2353–60.
- [131] Kuijlen JM, De Haan BJ, Helfrich W, de Boer JF, Samplonius D, Mooij JJ, et al. The efficacy of alginate encapsulated CHO-K1 single chain-TRAIL producer cells in the treatment of brain tumors. J Neurooncol 2006;78: 31–9.
- [132] King A, Strand B, Rokstad AM, Kulseng B, Andersson A, Skjak-Braek G, et al. Improvement of the biocompatibility of alginate/poly-L-lysine/alginate microcapsules by the use of epimerized alginate as a coating. J Biomed Mater Res 2003;64A:533–9.
- [133] Tan WB, Zhang Y. Surface modification of gold and quantum dot nanoparticles with chitosan for bioapplications. J Biomed Mater Res 2005;75A:56–62.
- [134] Robitaille R, Leblond FA, Henley N, Prud'homme GJ, Drobetsky E, Hall JP. Alginate-poly-L-lysine microcapsule biocompatibility: a novel RT-PCR method for cytokine gene expression analysis in pericapsular infiltrates. J Biomed Mater Res 1999;45:223–30.
- [135] Canaple L, Nurdin N, Angelova N, Saugy D, Hunkeler D, Desvergne B. Maintenance of primary murine hepatocyte functions in multicomponent polymer capsules – in vitro cryopreservation studies. J Hepatol 2001;34: 11–8.
- [136] Hurteaux R, Edwards Levy F, Laurent Maquin D, Levy MC. Coating alginate microspheres with a serum albumin-alginate membrane: application to the encapsulation of a peptide. Eur J Pharm Sci 2005;24:187–97.

- [137] Campioni EG, Nobrega JN, Sefton MV. HEMA/MMMA microcapsule implants in hemiparkinsonian rat brain: biocompatibility assessment using [3H]PK11195 as a marker for gliosis. Biomaterials 1998;19:829–37.
- [138] Luong Van E, Grondahl L, Nurcombe V, Cool S. In vitro biocompatibility and bioactivity of microencapsulated heparan sulfate. Biomaterials 2007;28:2127–36.
- [139] Orive G, Carcaboso AM, Hernandez RM, Gascon AR, Pedraz JL. Biocompatibility evaluation of different alginates and alginate-based microcapsules. Biomacromolecules 2005;6:927–31.
- [140] Juste S, Lessard M, Henley N, Menard M, Halle JP. Effect of poly-L-lysine coating on macrophage activation by alginate-based microcapsules: assessment using a new in vitro method. J Biomed Mater Res 2005;72A:389–98.
- [141] Abdel-Naby MA, Reyad RM, Abdel-Fattah AF. Biosynthesis of cyclodextrin glucosyltransferase by immobilized *Bacillus amyloliquefaciens* in batch and continuous cultures. Biochem Eng J 2000;5:1–9.
- [142] Muyima NYO, Cloete TC. Growth and phosphate uptake of immobilized Acinetobacter cells suspended in activated sludge mixed liquor. Water Res 1995;29:2461–6.
- [143] Toth D, Tomasovicova D, Gemeiner P, Kurillova L. Metabolic characteristics of bacterial cells entrapped in beaded calcium alginate and/or pectate gels. Folia Microbiol 1989;34:515–24.
- [144] Szczesna Antczak M, Galas E. Bacillus subtilis cells immobilised in PVA-cryogels. Biomol Eng 2001;17:55–63.
- [145] Zhang LY, Yao SJ, Guan YX. Effects of poly(methylene-co-guanidine) on microbial growth in an alginate/cellulose sulphate-CaCl<sub>2</sub>/poly(methylene-coguanidine) capsule system. Proc Biochem 2005;40:189–93.
- [146] Longo MA, Novella IS, Garcia LA, Diaz M. Comparison of *Bacillus subtilis* and *Serratia marcescens* as protease producers under different operating conditions. J Biosci Bioeng 1999;88:35–40.
- [147] Santos-Rosa F, Galvan F, Vega JM. Biological viability of *Chlamydomonas reinhardii* cells entrapped in alginate beads for ammonium photoproduction. J Biotechnol 1989;9:209–20.
- [148] Suzuki T, Yamaguchi T, Ishida M. Immobilization of *Prototheca zopfii* in calcium-alginate beads for the degradation of hydrocarbons. Process Biochem 1998;33:541–6.
- [149] Vilain S, Cosette P, Hubert M, Lange C, Junter GA, Jouenne T. Proteomic analysis of agar gel-entrapped *Pseudomonas aeruginosa*. Proteomics 2004;4:1996–2004.
- [150] Chen KC, Huang CT. Effects of the growth of *Trichosporon cutaneum* in calcium alginate beads upon bead structure and oxygen transfer characteristics. Enzyme Microb Technol 1988;10:284–92.
- [151] Willaert R, Baron G. Growth kinetics of gel-immobilized yeast cells studied by on-line microscopy. Appl Microbiol Biotechnol 1993;39:347–52.
- [152] Pashova S, Slokoska L, Sheremetska P, Krumova E, Vasileva M, Angelova M. Physiological aspects of immobilised Aspergillus niger cells producing polymethylgalacturonase. Process Biochem 1999;35:15–9.
- [153] Lohmeier Vogel EM, McIntyre DD, Vogel HJ. Phosphorus-31 and carbon-13 nuclear magnetic resonance studies of glucose and xylose metabolism in cell suspensions and agarose-immobilized cultures of *Pichia stipitis* and *Saccharomyces cerevisiae*. Appl Environ Microbiol 1996;62:2832–8.
- [154] Asanza Teruel ML, Gontier E, Bienaime C, Nava Saucedo JE, Barbotin JN. Response surface analysis of chlortetracycline and tetracycline production with K-carrageenan immobilized *Streptomyces aureofaciens*. Enzyme Microb Technol 1997;21:314–20.
- [155] Sonomoto K, Chinachoti N, Endo N, Ishizaki A. Biosynthetic production of nisin Z by immobilized *Lactococcus lactis* IO-1. J Mol Catalysis B Enzymatic 2000;10:325–34.
- [156] Angelova MB, Pashova SB, Slokoska LS. Comparison of antioxidant enzyme biosynthesis by free and immobilized *Aspergillus niger* cells. Enzyme Microb Technol 2000;26:544–9.
- [157] Jirku V. Whole cell immobilization as a means of enhancing ethanol tolerance. J Ind Microbiol Biotechnol 1999;22:147–51.
- [158] Cassidy MB, Shaw KW, Lee H, Trevors JT. Enhanced mineralization of pentachlorophenol by K-carrageenan-encapsulated *Pseudomonas* sp. UG30. Appl Microbiol Biotechnol 1997;47:108–13.
- [159] Annadurai G, Babu SR, Mahesh KPO, Murugesan T. Adsorption and biodegradation of phenol by chitosan-immobilized *Pseudomonas putida* (NICM 2174). Bioprocess Eng 2000;22:493–501.
- [160] Vilain S, Cosette P, Hubert M, Lange C, Junter GA, Jouenne T. Comparative proteomic analysis of planktonic and immobilized *Pseudomonas aeruginosa* cells: a multivariate statistical approach. Anal Biochem 2004;329:120–30.
- [161] Kumar PK, Schugerl K. Immobilization of genetically engineered cells: a new strategy for higher stability. J Biotechnol 1990;14:255–72.
- [162] Zaghloul TI, Hendawy HM, El Assar S, Mostafa MH. Enhanced stability of the cloned *Bacillus subtilis* alkaline protease gene in alginate-immobilized *B. subtilis* cells. Enzyme Microb Technol 2002;30:862–6.
- [163] Vehmaanpera JO, Korhola MP. Stability of the recombinant plasmid carrying the *Bacillus amyloliquefaciens* á-amylase gene in *B. subtilis*. Appl Microbiol Biotechnol 1986;23:456–61.
- [164] Huang J, Dhulster P, Thomas D, Barbotin JN. Agitation rate effects on plasmid stability in immobilized and free-cell continuous cultures of recombinant *E. coli*. Enzyme Microb Technol 1990;12:933–9.